

# Nacreous composite materials: an XFEM study for a broad understanding of the materials toughening mechanisms

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## Abstract

Biological materials have evolved through thousands of years, adapting, morphing, and optimizing to their particular function. One of the many natural materials that are widely studied is nacre, an elegant merge of stiff (mineral) and soft (biopolymer) components with extremely high mechanical properties, which are highly desired for structural applications. Naturally, nacre has been a source of inspiration for developing artificial composites with different levels of intrinsic designs. Some of these designs exploit the



microstructures of the materials, such as the connection between the composite stiffer parts, known as mineral bridges. To develop an eXtended Finite Element Method (XFEM)-based model of a biphasic composite inspired by the nacreous brick-and-mortar morphology, initially, we evaluate the use of XFEM on single materials models, including a hyperelastic material. Then, simulation of complex bioinspired materials shows that structures mimicking mineral bridges considerably improve composites' mechanical properties such as strength and toughness. The influence of the biomimetic mineral volume fraction on the overall toughening mechanisms, particularly crack arresting, is demonstrated. Our results provide a numerical approach to simulating biphasic materials with hyperelastic components and contrasting material properties (e.g., stiff and ductile) that have potential applications in complex composite structural designs.

**Keywords:** Fracture; Mechanical properties; Numerical analysis; XFEM; bioinspired composites.

## 1 **1. Introduction**

2 Natural materials are in constant self-improvement towards optimization of specialized  
3 functions such as antifouling [1, 2], thermal resistance [3], and aero drag reduction [4],  
4 allowing species to evolve and easier overcome environment elements and predators. The  
5 development of nacre is a specific case where shellfishes are shielded through a highly  
6 complex multiscale composite. Nacre combines two constituents to achieve remarkable  
7 material properties as a typical composite. A brick-and-mortar architecture is present at  
8 the nanoscale, where brick-shaped mineral platelets are embedded in an organic-  
9 polymeric matrix [5]. Nacre is extremely strong and tough, far exceeding the properties  
10 of its monolithic components. Moreover, the low-density constituents allow it to reach an  
11 extraordinary combination of lightness and toughness. The specific microstructure creates  
12 unique multiscale toughening mechanisms. For instance, crack deflection and arrest [6,  
13 7], mineral bridging [8-11], brick interlocking [12, 13], and viscoelastic adhesive  
14 behavior of the organic biopolymer [14-16]. Through controllable designs, nacreous  
15 inspired composite materials have been shown to experimentally replicate in engineering  
16 composites similar toughening mechanisms [17-20].

17 Theoretical models of the nacreous microstructure are well developed [21-23], but they  
18 cannot fully describe intricate nano- and micro-scale mechanisms. In the opposite  
19 direction, numerical models have attempted to solve the issue as they provide great  
20 versatility in studying multiple physical phenomena [24, 25]. Greco, Leonetti [26]  
21 developed a multiscale model that allowed the visualization of matrix cracking on nacre-  
22 like composites. Nevertheless, the solution requires complex user-input computations.  
23 Cohesive models [27, 28] showed less sophisticated yet accurate crack propagation  
24 analysis, but the proposed approach has a significant drawback: it cannot predict the crack  
25 initiation. Thus, the user selection of the crack location can alter the propagation  
26 massively.

27 The eXtended Finite Element Method (XFEM) is a numerical model mainly used in  
28 fracture mechanics analysis [29], with successful applications in simulating cracks in  
29 composites [30-34], natural [35-37], and bioinspired materials [38, 39]. Despite  
30 convergence issues, it can simulate the crack initiation combined with its propagation,  
31 describing the material mechanical behavior until total fracture. This primary advantage  
32 can significantly assist in observing cracks in materials with complex microstructures  
33 such as nacre. In this direction, XFEM has been applied to predict the behavior of bone-

34 inspired composites, showing good agreement between simulated and experimental crack  
35 propagation results [39, 40]. The application of XFEM to nacre-inspired composites is  
36 not widely established [41]. Le, Ghazlan [41] created conch-inspired 3D-printed materials  
37 and validated their behavior with XFEM. They changed the printing nozzle path to create  
38 different material orientations that resemble aragonite distribution found on conch  
39 materials and evaluated the crack propagation with XFEM. The occurrence of mineral  
40 bridging was not studied.

41 Nacre mineral bridges (MBs) have recently been in the spotlight [27, 42-46] because the  
42 mineral interconnections between rigid platelets can considerably increase the composite  
43 strength and toughness. Gu, Libonati [10] fabricated nacre-like composites through 3D-  
44 printing with different volume fractions of MBs, showing the influence of MBs on the  
45 material mechanical properties. By solely increasing the MBs fraction, the strength of the  
46 composites directly rises. However, the toughness is increased only until a threshold and  
47 declines afterwards. The influence of the MBs on the stress field was partially analyzed  
48 through finite element modeling and comparison with strain fields obtained from digital  
49 image correlation. Yet, crack propagation has not been numerically investigated.  
50 Askarinejad and Rahbar [44] showed that MBs and nano-asperities in the nacre platelets  
51 directly affect the material mechanical behavior. These nano-scaled features with near  
52 theoretical strength create a highly nonlinear material behavior. Moreover, the waviness  
53 of the platelets [45], and the organic matrix region in the proximity of MBs [46] can also  
54 influence the nacre behavior to exterior stresses.

55 In this work, bioinspired composites are modeled through XFEM to mimic the specific  
56 toughening mechanisms observed in nacre. The geometrical and material parameters  
57 followed previous studies [10, 47, 48], and additional experimental testing was carried  
58 out to support the data. Numerical analyses of tensile and fracture tests of brick-and-  
59 mortar composites were developed to observe the microstructural response to external  
60 loading, aiming at the fracture behavior. These models were divided into two main groups,  
61 (i) with and (ii) without mineral bridges (MBs), and categorized by their stiff component  
62 volume fraction: 50%, 60%, and 70%. Results showed that our XFEM models could  
63 predict experimental results with good agreement, especially for models without MBs.  
64 Moreover, the simulations showed that MBs were able to arrest cracks, highlighting the  
65 MBs pivot role in increasing the material mechanical properties such as toughness and  
66 strength. Our work showed that an XFEM-based modeling approach can represent a

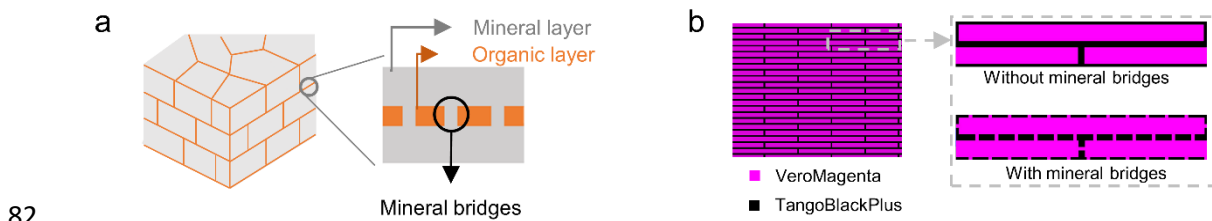
67 useful framework for designing bioinspired composites with advanced microstructural  
68 features, such as the inclusion of material interconnections replicating MBs.

69

## 70 2. Material and Methods

### 71 2.1. Materials design

72 Inspired by the brick-and-mortar structure (**Figure 1a**), our composite design (**Figure 1b**)  
73 is made of two constituents: VeroMagenta (VM) and TangoBlackPlus (TBP). VM  
74 represents the stiffer part of the composite, making up the aragonite phase in the natural  
75 counterpart. TBP is a soft-hyperelastic material, portraying the organic role played by  
76 nature. These materials were chosen as they can be together implemented into a multi-  
77 material commercial 3D printer (Objet500 Connex3, USA). Their material properties  
78 have been previously determined and described by Libonati and Gu [10, 47, 48]. To  
79 support the development of the hyperelastic model for TBP, a bi-axial tensile test was  
80 carried out. Numerical modeling of both the base materials and the composite materials  
81 was performed.



83 **Figure 1.** (a) Nacre microstructure highlighting the aragonite mineral phase (in grey) and  
84 the biopolymeric organic layer (in orange), and the spatial locations of mineral bridges,  
85 connecting adjacent aragonite platelets across the biopolymer. (b) Overview of the  
86 bioinspired composite, made by 3D-printed materials: VeroMagenta (VM), mimicking  
87 the nacreous mineral phase, and TangoBlackPlus (TBP), as the biopolymeric organic  
88 layer. The composite has unit cells with or without bioinspired mineral bridges.

89

### 90 2.2. Experimental testing: bi-axial testing

91 Force-controlled biaxial tests were performed in a custom-made setup with appropriate  
92 specimen dimensions (**Figure S1**) necessary due to the absence of bi-axial test standards  
93 [49]. The setup consists of four linear actuators that can apply independent displacements

94 with submicron resolution (**Figure S1a and S1b**). The test speed was 6 mm/min to reduce  
95 the viscoelastic effect found in rubber-like materials. The specimens have a cruciform  
96 geometry with slits in the arms to facilitate the load transfer (**Figure S1c and S1d**). The  
97 local strain levels were measured by digital tracking marks added to the specimen surface.  
98 Bi-axial results were used as input to the simulations and can be seen in the Supporting  
99 Information (**Figure S1e**).

### 100 *2.3. Numerical modeling of base materials*

101 The development of computational models replicating the uniaxial tests of single  
102 materials, VM and TBP, was the base to further create a more complex composite model.  
103 The XFEM is an extension of the conventional Finite Elements Method (FEM) and is  
104 used to solve fracture mechanics problems. The most convenient advantage of the XFEM  
105 is that the user does not necessarily need to set the crack initiation location. The method  
106 creates a crack when a few conditions are established, being the most disseminated when  
107 the local principal stress is higher than the material maximum principal stress (MAXPS).  
108 The crack propagation direction follows the damage evolution parameters. In our case,  
109 the crack is directed to a neighboring element from its start location when an element is  
110 under a local displacement higher than the threshold (e.g., maximum strain multiplied by  
111 the characteristic mesh element length). The procedure is repeated until the crack cannot  
112 propagate anymore, either due to a total failure or the non-achievement of local crack  
113 propagation conditions. Tensile and fracture tests were simulated using the software  
114 Abaqus 6.14.

115 - The 2D dog-bone tensile test geometry followed the experimental standard (**Figure**  
116 **S2a**). The model was constrained in the left section and had a positive displacement in  
117 the right section while constrained in the y-axis. The mesh comprehended 6528 CPS4R  
118 (linear quadrilateral plane stress with reduced integration) elements with coarse mesh  
119 in the extremities and more refined in the samples neck region, reached after a mesh  
120 sensitivity analysis (**Figure S2b and S2c**).

121 - The fracture test geometry had a square-shaped configuration (80 x 80 x 3 mm), with  
122 a 16 mm lateral notch, represented in the simulation by a wire-type geometry (**Figure**  
123 **S3a**). The model had a total of 9100 CPS4R elements, obtained after a mesh sensitivity  
124 analysis (**Figure S3b and S3c**).

125 The input VM material properties followed Libonati, Cipriano (42), (43) in both models.  
 126 A biaxial tensile test was performed to obtain additional information for the hyperelastic  
 127 material (i.e., TBP), allowing a more accurate definition of the material model. The  
 128 experimental results were compared to three numerical results run with different  
 129 hyperelastic models: Arruda-Boyce, Ogden, and Polynomial. The Arruda-Boyce model  
 130 [50] represents the material as a cubic element containing eight chains, with material-  
 131 dependent three variables:  $\mu$ ,  $\lambda$ , and  $D$ . The Arruda-Boyce strain energy potential is  $U =$   
 132  $U(\mu_0, \mu, \lambda, D)$ . However, at moderate strain, the accuracy of the model is not great [51].  
 133 The second-order polynomial model (Poly2) is based on the left Cauchy-Green  
 134 deformation tensor, where  $U = U(D_1, D_2, C_1, C_2, C_{10}, C_{11}, C_{20})$ , but often overestimates  
 135 the material properties [52]. The Ogden model is a model founded on the Helmholtz free  
 136 energy. Its third-order strain energy is  $U = U(\mu_1, \mu_2, \mu_3, \alpha_1, \alpha_2, \alpha_3, D_1, D_2, D_3)$ . Despite  
 137 having great accuracy, the model stability is very influenced by the input parameters [53].  
 138 The applied variables for the three models in the tensile test for single components are  
 139 described in **Table 1**. In the fracture test simulations, the model adopted was Ogden3,  
 140 followed by the results from the tensile tests.

141 **Table 1.** Coefficients adopted for the hyperelastic models.

Model	Coefficients			
Arruda-Boyce	$\mu = 0.1373$	$\mu_0 = 0.1617$	$\lambda = 2.0821$	$D = 1.2370 \cdot 10^{-3}$
	$\mu_1 = -52.2138$	$\mu_2 = 26.0840$	$\mu_3 = 26.2620$	
Ogden3	$\alpha_1 = 1.0758$	$\alpha_2 = 1.2509$	$\alpha_3 = 0.8996$	
	$D_1 = 1.5097 \cdot 10^{-3}$	$D_2 = 0.0000$	$D_3 = 0.0000$	
Poly2	$D_1 = 0.2358$	$D_2 = 0.0000$	$C_1 = 0.0003$	$C_2 = -0.0110$
	$C_{10} = 0.8510$	$C_{11} = 0.0288$	$C_{20} = -0.0073$	

142

#### 143 2.4. Numerical models of nacre-like composite

144 The unit cells followed three configurations, with 50%, 60%, and 70% VM volume  
 145 fractions. Detailed dimensions (**Figure S4a**) are available in **Table S1**. Displacement  
 146 conditions were applied to the two lateral edges, while symmetric boundary conditions  
 147 were set to the others to replicate the presence of adjacent cells (**Figure S4b**). The  
 148 component material properties are shown in **Table 2**. The configuration has 13850 four-  
 149 node plane stress elements (CPS4R) with hourglass control. Hourglass control was

150 adopted to overcome excessive distortion inherent to TBP material behavior. Mesh  
 151 dependency analysis is shown in **Figure S4c**. Analyses were run with a maximum number  
 152 of cutbacks allowed for an increment (IA) of 20. The results of the numerical models  
 153 were compared to experimental data available in a previous publication [10], where  
 154 authors studied the influence of bridging in nacre-inspired composites varying the stiff  
 155 volume fraction content (i.e. VM). The samples contained an edge crack in the design and  
 156 were 3D printed using a multi-material printer (Objet500 Connex3, Stratasys).  
 157 Experimental testing was performed under displacement-controlled tension in a universal  
 158 testing machine at a 2 mm/min extension rate [10].

159

160 **Table 2.** Material properties adopted to model TBP and VM.

Parameter	TBP	VM
Maximum principal stress	0.73 MPa	54.30 MPa
Displacement at fracture	0.5275 mm	0.0112 mm
Damage stabilization coefficient	$1 \cdot 10^{-6}$	$1 \cdot 10^{-4}$
Elastic modulus	-	2183.4 MPa
Hyperelastic model	Ogden 3	-
Poisson's ratio	0.49	0.35

161

### 162 3. Results

#### 163 3.1. Results for the homogeneous materials

164 For the TBP tensile test, computational results showed two cracks in mirrored positions  
 165 in the region where the sample neck finishes. The cracks propagated equally, fracturing  
 166 the specimen in two parts. Similar fracture behavior was described for the experimental  
 167 result (**Figure 2a**). The three hyperelastic models showed good agreement with the  
 168 experimental result in the uniaxial tensile test (**Table 3**). The Arruda-Boyce  
 169 overestimated the strength by 8.4%, and the polynomial underestimated by 6.4%. The  
 170 Poly2 model showed repeated convergence issues during computation, despite the small  
 171 strength variation. Thus, the Ogden3 model was selected as the most adequate  
 172 hyperelastic model for the TBP component.

173

174 **Table 3.** Strength comparison between the hyperelastic models and experimental for the  
175 TBP material under uniaxial tensile conditions.

Result	Strength [MPa]	Difference
Experimental	0.7373	-
Arruda-Boyce	0.7993	8.4%
Ogden3	0.7464	1.2%
Poly2	0.6902	-6.4%

176

177 Similarly, the fracture test replicated well the observed behavior, validating the choice for  
178 the Ogden3 hyperelastic material model (**Figure 2b**). The crack propagated  
179 perpendicularly from the test displacement, growing horizontally until total fracture. The  
180 numerical analysis showed a material strength of 0.112 MPa and a strain at fracture of  
181 33.7%, closely comparable to the experimental results of 0.107 MPa and 37.0%.

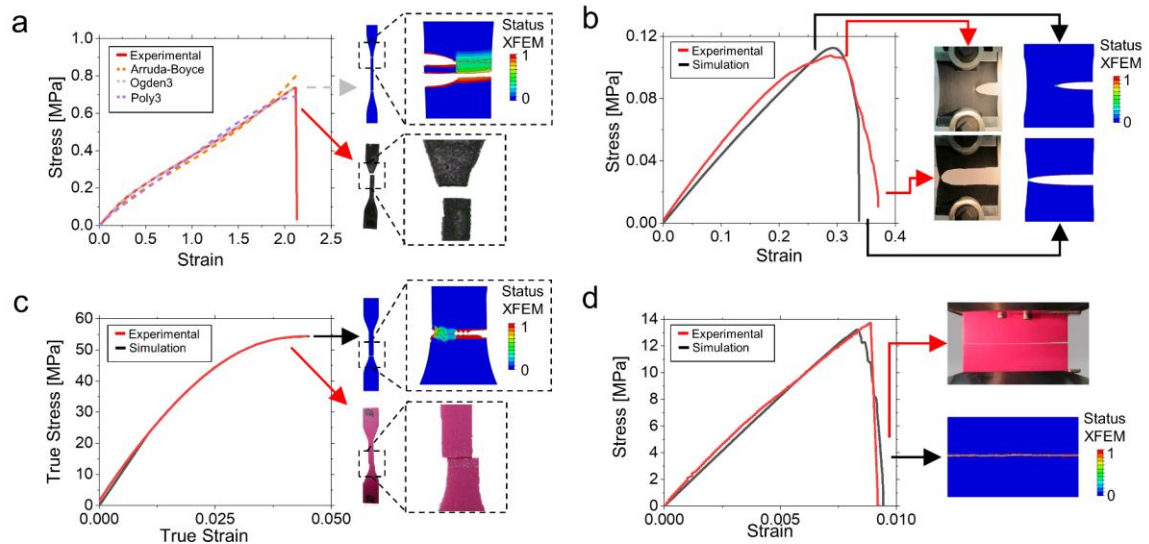
182 The tensile test results for VM showed the same failure mode as the experimental test: a  
183 crack started in the extremity of the sample neck region and led to the sample failure  
184 (**Figure 2c**). The difference between the experimental and numerical material strength  
185 and stiffness was minimal, 0.02% and 3.45%, respectively (**Table 4**). For the fracture test,  
186 the crack continued from the predetermined initial location and propagated horizontally  
187 (**Figure 2d**). The numerical maximum stress was 13.74 MPa, 3.9% higher than the  
188 experimental value (*i.e.*, 13.22 MPa). The failure modes of the tensile and fracture tests  
189 were identical to the reported experimentally (**Figure 2c and 2d**).

190

191 **Table 4.** Strength comparison between the numerical and experimental for VM material  
192 under uniaxial tensile conditions.

Result	Strength [MPa]	Elastic modulus [MPa]
Experimental	54.37	2112.97
Numerical	54.36	2185.85
Difference	0.02%	3.45%

193



194

195 **Figure 2.** (a) Comparison between the experimental and XFEM results for the (a, c)  
 196 uniaxial tensile and (b, d) fracture test of (a, b) TangoBlackPlus and (c, d) VeroMagenta.  
 197 Status XFEM states the local crack propagation, being a fully propagation, thus total  
 198 element fracture, represented in red (Status XFEM=1), and blue the opposite (Status  
 199 XFEM=0) [47].

200

### 201 3.2. Results for the bioinspired composites

202 The numerical models were evaluated according to their experimental counterparts. For  
 203 the models without MBs, the accuracy varied with respect to the VM volume fraction  
 204 (**Table 5**). The models with 50% and 60% had a high (*i.e.*, up to 48%) deviation from the  
 205 experimental strength, determined as the maximum stress. On the contrary, the 70%  
 206 model deviated only 0.68% from its experimentally measured strength value. For the  
 207 toughness, calculated as the area underneath the stress-strain curve (until strain at rupture),  
 208 the models were able to replicate the experimental behavior with a satisfactory accuracy  
 209 (*i.e.*, between -8% to 9%). An increase in the VM fraction enhanced maximum strength  
 210 but decreased strain at fracture, maintaining the toughness values within very similar  
 211 ranges (**Figure 3a-c**). Overall, the results showed that XFEM was able to predict the  
 212 composite mechanical properties with reasonable accuracy. In the three models, the upper  
 213 VM platelet arrested the crack tip and an axial stress (S11) concentration at the tip was  
 214 present (**Figure 4a**). On the contrary, the lower platelets had higher shear stress (S12) and  
 215 maximum absolute principal stress (MAXPS-AB) localized at the extremities furthest  
 216 from the crack tip (**Figure 4b-c**).

217

**Table 5.** Evaluation of the numerical models without MBs.

Result	50% VM		60% VM		70% VM	
	Strength [MPa]	Toughness [MJ/m <sup>3</sup> ]	Strength [MPa]	Toughness [MJ/m <sup>3</sup> ]	Strength [MPa]	Toughness [MJ/m <sup>3</sup> ]
Experimental	2.29	0.206	2.29	0.179	4.4	0.236
Numerical	2.95	0.215	3.37	0.194	4.43	0.219
Difference	28.82%	4.36%	47.16%	8.37%	0.68%	-7.20%

218

219

**Table 6.** Evaluation of the numerical models with MBs.

Result	50% VM-MB		60% VM-MB		70% VM-MB	
	Strength [MPa]	Toughness [MJ/m <sup>3</sup> ]	Strength [MPa]	Toughness [MJ/m <sup>3</sup> ]	Strength [MPa]	Toughness [MJ/m <sup>3</sup> ]
Experimental	5.96	0.358	6.72	0.363	8.77	0.41
Numerical	13.15	0.818	11.97	0.748	12.29	0.53
Difference	120.63%	128.49%	78.12%	106.06%	40.13%	29.26%

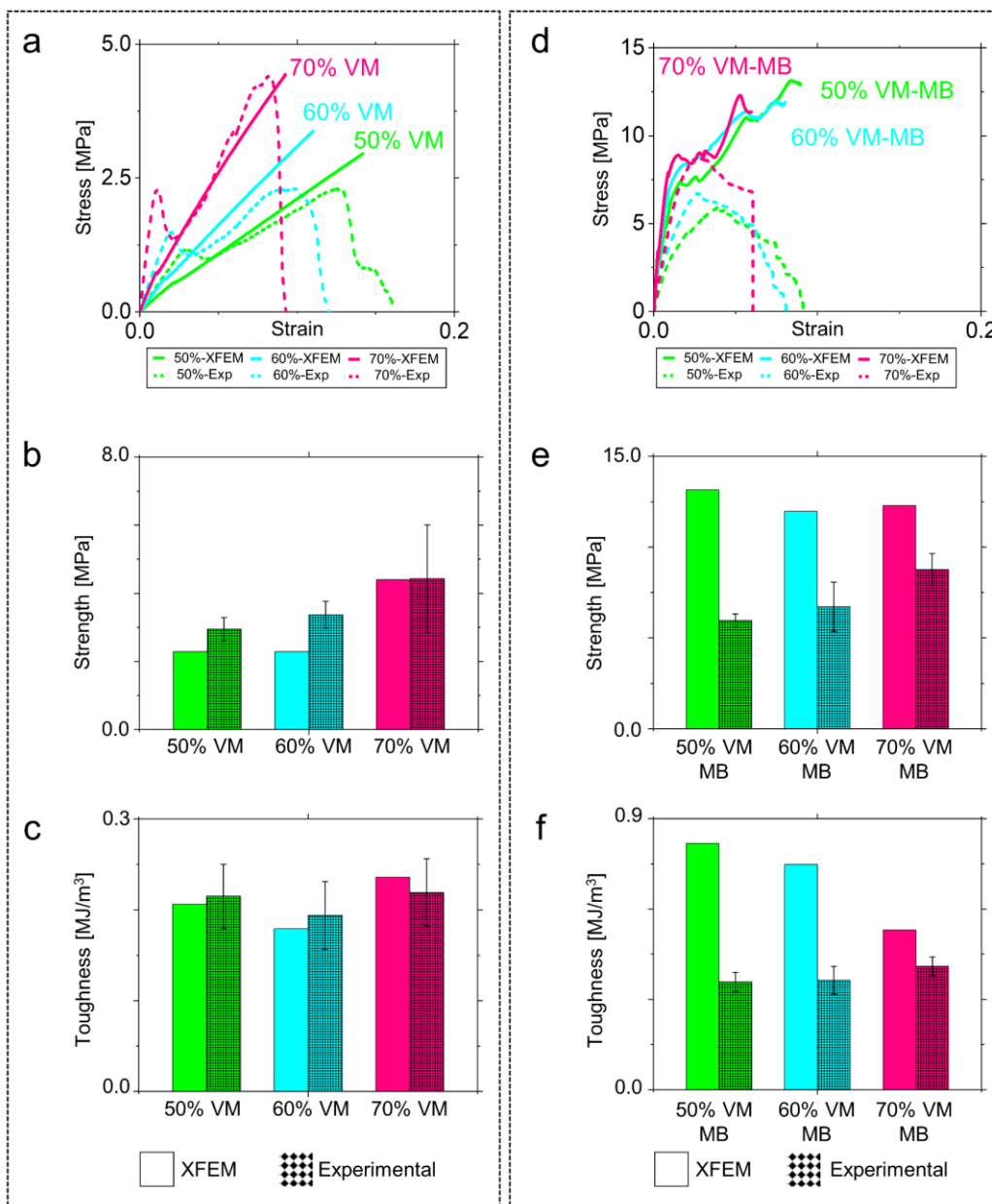
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221 For the models with MBs, the quantitative comparison revealed high deviation for both  
 222 strength and toughness (**Table 6**), in particular for models with a low VM volume fraction,  
 223 such as the 50% VM-MB (**Figure 4f**). Such models showed high stress concentration,  
 224 which accentuates the occurrence of computational issues (*e.g.*, convergence issues and  
 225 distorted elements), enlarging the gap between numerical and experimental results. The  
 226 model with the stress-strain curve most similar to its experimental counterpart had the  
 227 highest VM fraction (*i.e.*, 70%) (**Figure 3d**).

228 Compared to their counterpart without MBs, all models with MBs showed a stiffer  
 229 behavior (**Figure 4g, h**). Naturally, this is due to the platelet bridging, acting as an  
 230 additional feature and enhancing stiffness during strained conditions. This is clear in all  
 231 three samples, where the MBs in the middle sections have the highest compression  
 232 stresses (**Figure 4d**). The strongest composite was the sample with 50% VM, but the  
 233 variation compared to the 60% and 70% VM is low (**Figure 4h**).

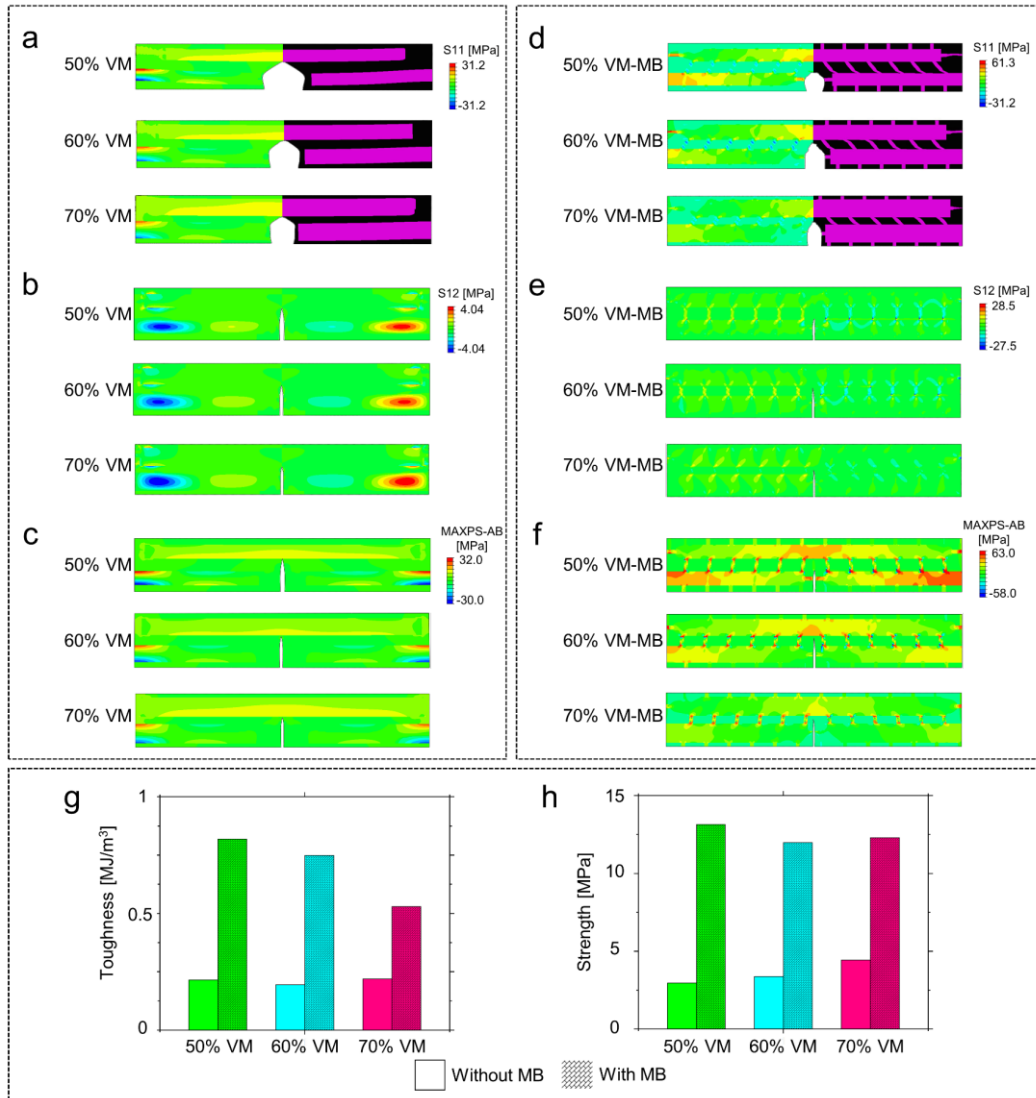
234 Regarding the shear stress response, for 50% and 60% VM, the highest absolute stresses  
 235 are located in the MBs. Meanwhile, for 70% VM, they were in the VM platelets, more

236 specific on the region in contact with the MBs (**Figure 4e**). The stress fields are different  
 237 for the maximum absolute principal stresses (MAXPS-AB) (**Figure 4f**). The model with  
 238 the lowest mineral fraction (*i.e.*, 50%) has higher MAXPS-AB in the platelets. On the  
 239 contrary, in the model with 70% VM, the MAXPS-AB peaks are in the mineral bridges.  
 240 This change in stresses could be the reason for the material lower toughness (**Figure 4g**).  
 241 The crack propagation analyses reconfirm the role of the bridging (**Figure 5**). For all  
 242 models with MB, between steps ii-iv, the stresses are intensified between the  
 243 bridge/platelet regions (**Figure 5d-e**), a clear contrast to their counterparts without MB  
 244 (**Figure 5a-c**).



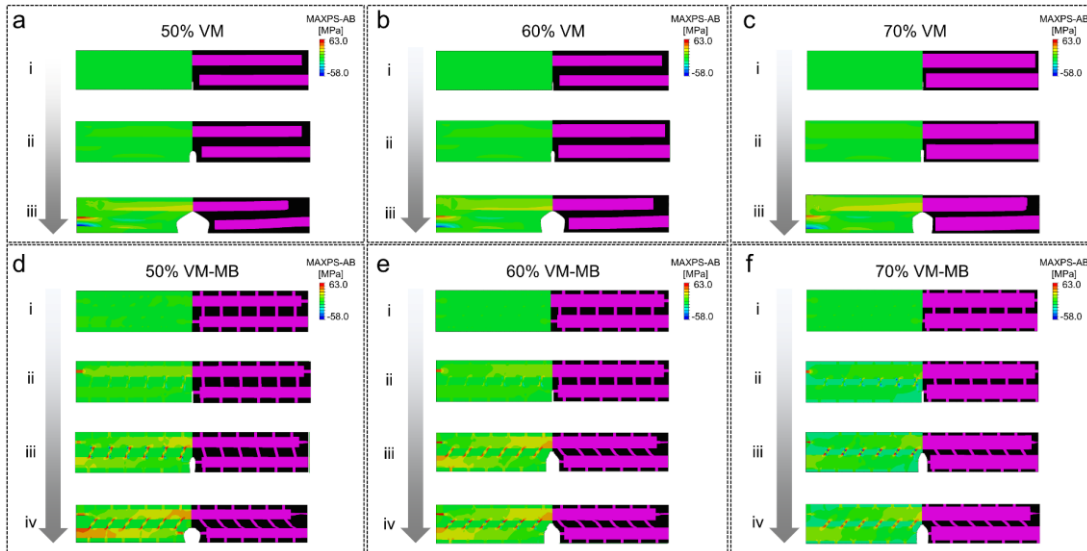
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246 **Figure 3.** Summarized comparison between the XFEM and experimental results for the  
 247 models (a-c) without MBs and (d-f) with MBs. (a) Stress-strain curves. (b) Strength and  
 248 (c) toughness bar plots.



249

250 **Figure 4.** Mechanical behavior of unit cells (a-c) without and (d-f) with MBs.  
 251 Comparison between (g) toughness and (h) strength for the unit cells, showing that the  
 252 inclusion of MBs enhance drastically the mechanical properties.



253

254 **Figure 5.** Crack propagation for models with (a, d) 50% VM, (b, e) 60% VM, and (c, f)  
 255 70% VM, (a-c) without and (d-f) with mineral bridging. The maximum absolute principal  
 256 stresses are shown for progressing steps (i-iv) for each configuration.

257

#### 258 4. Conclusions

259 In this work, we evaluated the application of XFEM as a method to simulate mechanical  
 260 properties on a composite material with complex geometry and hyperelastic elements. By  
 261 studying bioinspired nacreous designs with and without mineral bridging, we showed the  
 262 capacity of XFEM to simulate failure in materials with hyperelastic behavior such as TBP.  
 263 The support of previous works allowed a comparison with respect to the experimental  
 264 results, validating the importance of mineral bridging on brick-and-mortar  
 265 microstructures. Together with toughness mechanisms of these structures, such as crack  
 266 arresting on tougher platelets, our analyses found that bridging plays a significant role in  
 267 the composite mechanical properties, especially because the MBs features act as  
 268 sacrificial bonds, allowing energy release when the composite is bearing loads. The  
 269 XFEM results showed higher strength and toughness for models with bridging when  
 270 compared to their opposite counterpart (*e.g.*, without bridging). This trend is in agreement  
 271 with the experimentally obtained results [10]. The influence of the additional platelet  
 272 connection depends intensely on the dimensions of the bridges. In this work, the volume  
 273 fraction of the stiffer element was chosen as a variable. For models without MBs, a higher  
 274 volume fraction resulted in a much lower toughness, but insignificant strength alteration.  
 275 Meanwhile, for the models with MBs, the increase of volume fraction raised the material

276 strength without considerable variation of toughness. For models with MBs and low VM  
277 volume fraction, a larger gap between experimental and computational results was seen,  
278 possibly due to high stress concentration that led to distorted elements and convergence  
279 issues. Our work showed that XFEM can be applied to simulate the failure of composite  
280 materials including a hyperelastic component with adequate accuracy and can be used as  
281 guidelines to design bioinspired composites that want to replicate mineral bridging.

282

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### 287 **Declaration of interest statement**

288 The authors declare no conflict of interest.

289

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### 293 **Author contributions**

294 **Andres Aguilar:** Investigation, Methodology, Formal analysis, Software, Writing -  
295 original draft. **Andre Vellwock:** Formal analysis, Visualization, Writing - original draft.  
296 **Andrea Avanzini:** Investigation. **Flavia Libonati:** Conceptualization, Investigation,  
297 Writing – Reviewing and Editing, Supervision.

298

### 299 **Data availability statement**

300 Data available on request.

301

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## Supplementary Information

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### 440 **Nacreous composite materials: an XFEM study for a broad** 441 **understanding of the materials toughening mechanisms**

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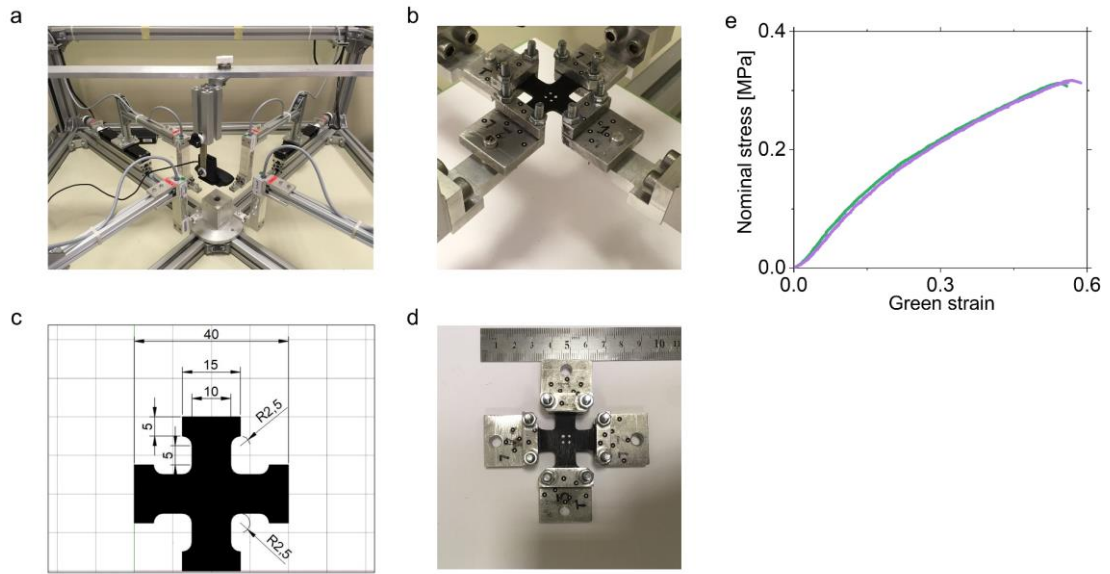
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456 **Figure S1.** (a) Bi-axial tensile test setup with (b) custom-made sample attached. (c)  
 457 Dimensions of the specimen. (d) Overview of the clamped sample. (e) Results of the bi-  
 458 axial testing; each curve is relative to straining direction.

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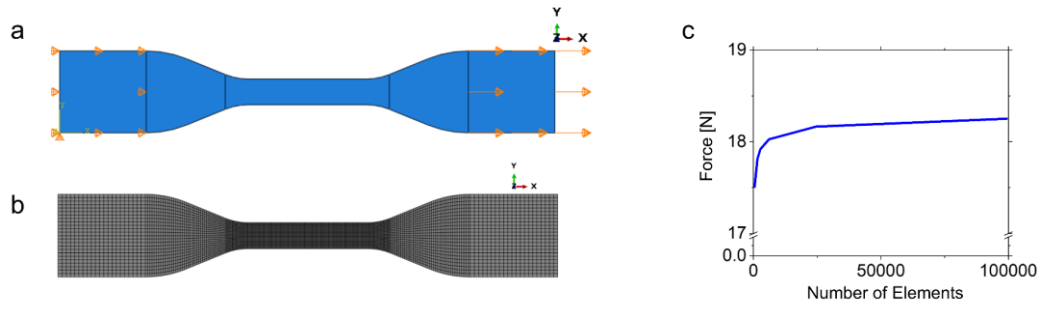
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469 **Figure S2.** Numerical analysis of the tensile test, which is (a) fixed at one end and strained  
 470 in the x-axis at the other, with (b) a more refined mesh in the sample's central region. (c)  
 471 Mesh sensitivity analysis.

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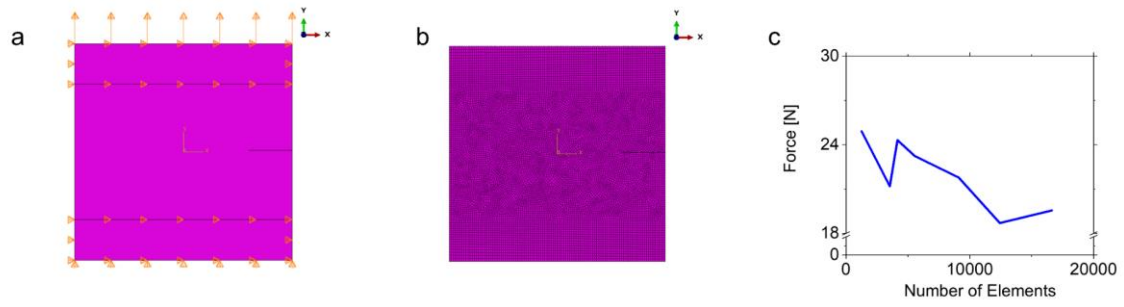
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490 **Figure S3.** Numerical analysis of the fracture test showing the (a) boundary conditions,  
 491 (b) general mesh, and (c) mesh sensitivity analysis.

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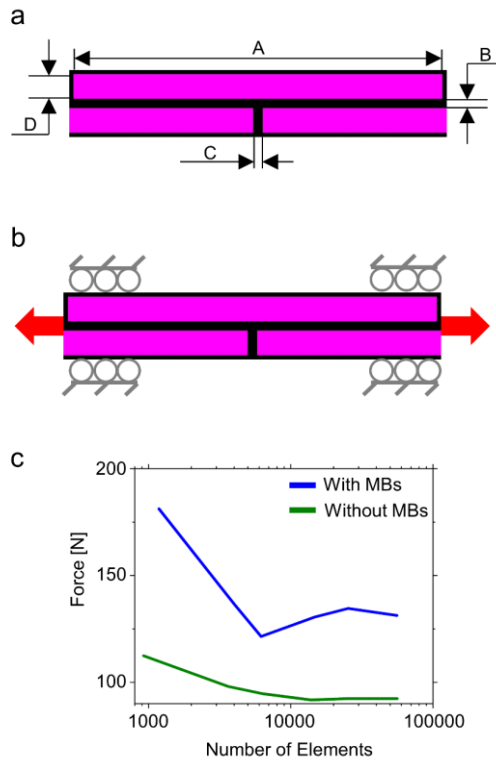
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504 **Figure S4.** (a) Dimensioning of the unit cells. (b) Boundary conditions applied to the  
 505 models. (c) Mesh sensitivity analysis for the models with and without MBs.

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**Table S1.** Model dimensions for the unit cells.

Dimensions [mm]	50% VM	60% VM	70% VM
A	14.39	14.65	14.85
B	0.64	0.51	0.38
C	0.85	0.59	0.39
D	0.72	0.85	0.98

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