



Extended Abstract Application of a Micro-Machined Electronic Nose to Detect Escherichia Coli in Human Urine Samples ⁺

Matteo Soprani 1,2,*, Giulia Zambotti 1,2, Emanuela Gobbi 2,3 and Andrea Ponzoni 1,2

- ¹ Department of Information Engineering, University of Brescia, Via Branze 38, 25123 Brescia, Italy; g.zambotti@unibs.it (G.Z.); a.ponzoni@unibs.it (A.P.)
- ² National Institute of Optics (INO), National Research Council (CNR), Via Branze 45, 25123 Brescia, Italy; e.gobbi@unibs.it
- ³ Department of Molecular and Translational Medicine, University of Brescia, Viale Europa 11, 25123 Brescia, Italy
- * Correspondence: m.soprani001@unibs.it
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1. Introduction

The analysis of volatile organic compounds (VOCs) as disease biomarkers released by the urine, it permits an early and non-invasive diagnosis of Urinary Tract Infections (UTI) [1]. For this purpose, an instrumental method like the electronic nose composed by micromachined metal oxide gas sensors has been taken under consideration. *Escherichia coli* (*E.coli*) is the pathogenic microorganism responsible for up to 80% of theUTI and it is here chosen as benchmark bacterium [2]. The purpose of this research work is to test the capability of the electronic nose approach to recognise the presence of *E.coli*, identificative of a possible UTI disturb [3], in urine samples.

2. Materials and Methods

In the research's work, a device named miniMOx (JLM Innovation, Tübingen, Germany) has been involved. It is equipped with two micromachined metal oxide gas sensors (MOX): TGS8100 (Figaro, Arlington Heights, IL, USA) and CSS801 (AMS, Premstaetten, Austria). The MOX are capable to work with custom temperature modulation protocols controlled though their embedded heaters. This modulation periodically activates and freezes the interaction between gaseous molecules and the metal oxide surface, producing a periodic resistance vs. time curve as a response. In particular, a square wave of a 20 seconds period was applied. A warm semi-period was settled at voltage of Vheaters: 2.31 V for 10 seconds while the cold one at the voltage of Vheater = 1.65 V for the same amount of time. The resistance vs. time curves obtained were described through the Δ Rcold-hot, Δ Rcold and Δ Rhot parameters. The Δ Rcold-hot represents the subtraction between the sensor's resistance measured at the end of the cold period and the resistance measured at the start of the warm period after 0.2 seconds. Δ Rcold signifies the difference between the sensor's resistance measured at the end of the cold period and after 0.2 seconds or at the beginning to the same period. Δ Rhot respects the warm period. In the end, a Principal Component Analysis algorithm (PCA function on Matlab) was used to elaborate the data acquired with the described parameters. Three representative samples were taken under consideration: urine, urine contaminated with a pathogenic microorganism (Escherichia coli) and sterilized water as a control. The analysis' procedure provided to place in contact the miniMOx for a time of 5 minutes with the head- space released from the samples, interspersed with 10 minutes for the sensors' recovery in ambient air. In parallel, bacterial counts were performed to monitor the Escherichia coli concentration during the whole analysis.

3. Results and Discussion

A summary of the obtained results is reported in the Figure 1.



Figure 1. Resistance vs. time curves obtained with the CSS801 sensor. Two cycles of a cold and warm semi-period recorded during the exposition to the VOCs released by urine's samples (**A**). Two cycles of a cold and warm semi-period recorded during the exposition to the VOCs released by urine contaminated with *E. coli* samples (**B**). A Principal Component Plot of the MOX sensors response to the VOCs released by water (blue circles), urine (black stars) and urine with *E. coli* (green crosses) (**C**).

From the Figure 1, it is possible to observe the resistance vs. time curves acquired with the CSS801 sensor during the exposition at the VOCs released by uncontaminated urine (Figure 1A) and urine inoculated with *E. coli* at the initial concentration of 104 CFU/ml (Figure 1B). The resistance values are lower during the warm semi-period and larger during the semi-cold one, mainlydue to thermal effect on the MOX semiconductor. The shape of these curves is sensitive to the surrounding atmosphere, with differences that can be properly resumed in terms of Δ Rcold-hot and Δ Rcold. PCA algorithm applied to the parameters explained before, leaded to results shown the Figure 1C. The PCA Score Plot represents a scenario with three different clusters. The blue circles for sterilized water, the black stars for the urine and the green crosses for the urine contaminated with *Escherichia coli*. It is possible to understand that there is a separation between the samples among the PC1 and PC2 aces. In particular, there is a separation between the two urine's samples. Since the difference between the two urine's samples is the *E. coli* presence, potentially the pathogenic microorganism is the responsible to the separation itself.

4. Conclusions

The custom measurement protocol developed with the commercial electronic nose miniMOx revealed suitable to discriminate between water, urine and urine with *E. coli* through the analysis of the VOCs released by them. Since *E. coli* causes different kind of diseases in the human body, an early detection of this pathogenic microorganism into the urine could prevent the illnesses development. In conclusion, the miniMOx could be an easy-to-use, low-cost device for the pre-screening diseases through the VOCs released by urine.

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